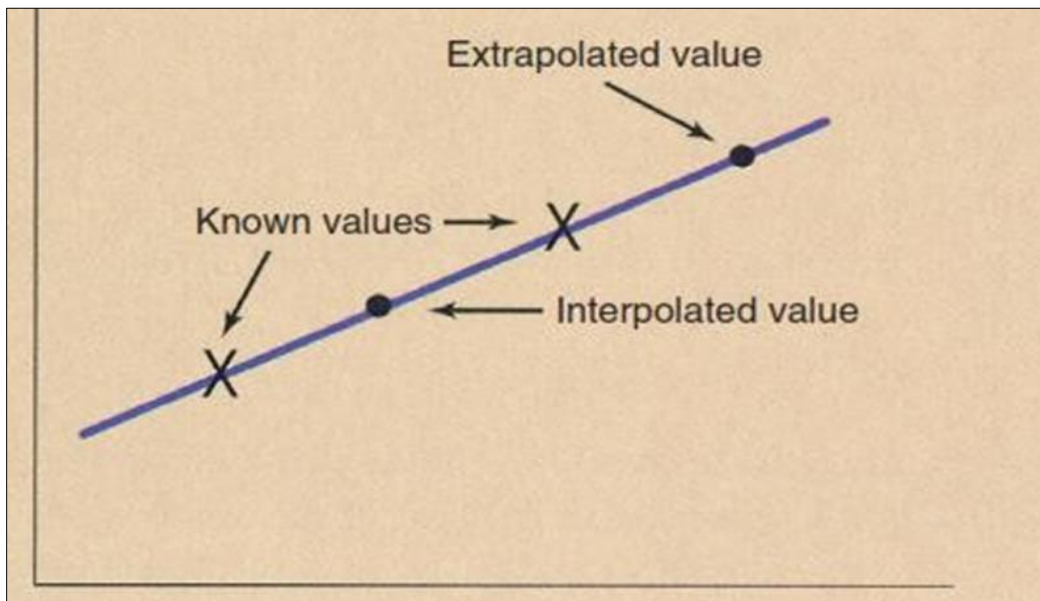


## Interpolation Algorithms

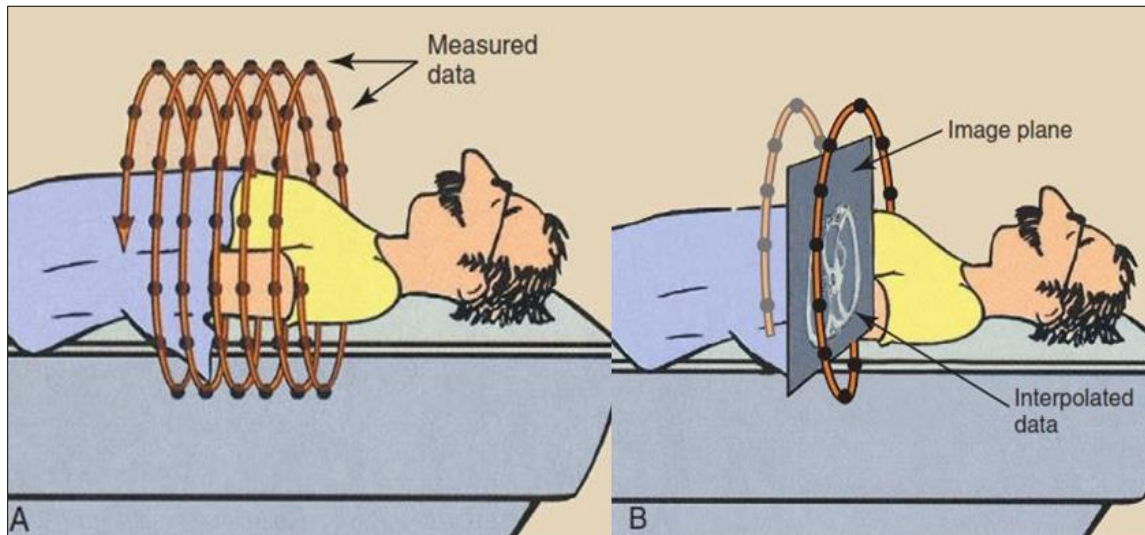
*Reconstruction of an image at any z-axis position* is possible because of a mathematical process called *interpolation*. **Figure (1)** presents a graphic representation of interpolation and extrapolation. If one wishes to estimate a value between *known values* that is an *interpolation*; if one wishes to estimate a value *beyond the range* of known values that is an *extrapolation*.



**Fig(1): Interpolation estimates a value between two known values. Extrapolation estimates a value beyond known values.**

During *helical CT*, image *data are received continuously*, as shown by the data points in Figure 2 A. When an image is reconstructed, as in Figure 2 B, the plane of the image does not contain enough data for reconstruction.

The data in that plane must be estimated by interpolation. Data interpolation is performed by a special computer program called an *interpolation algorithm*.

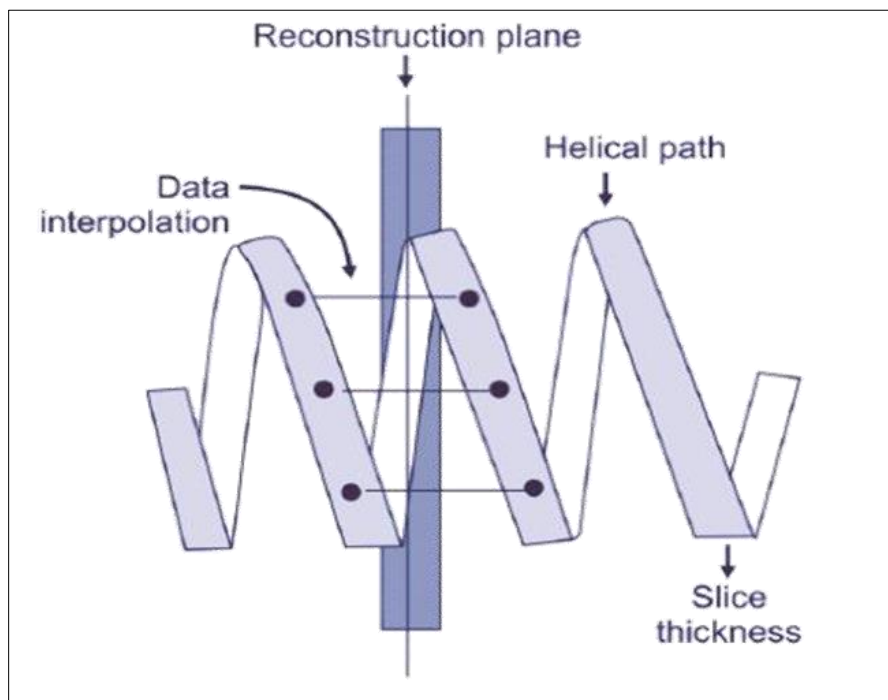


**Fig. (2): A, During multislice helical computed tomography, image data are continuously sampled. B, Interpolation of data is performed to reconstruct the image in any transverse plane.**

Image *interpolation creates a number of new slices between known slices* in order to obtain an isotropic volume image.

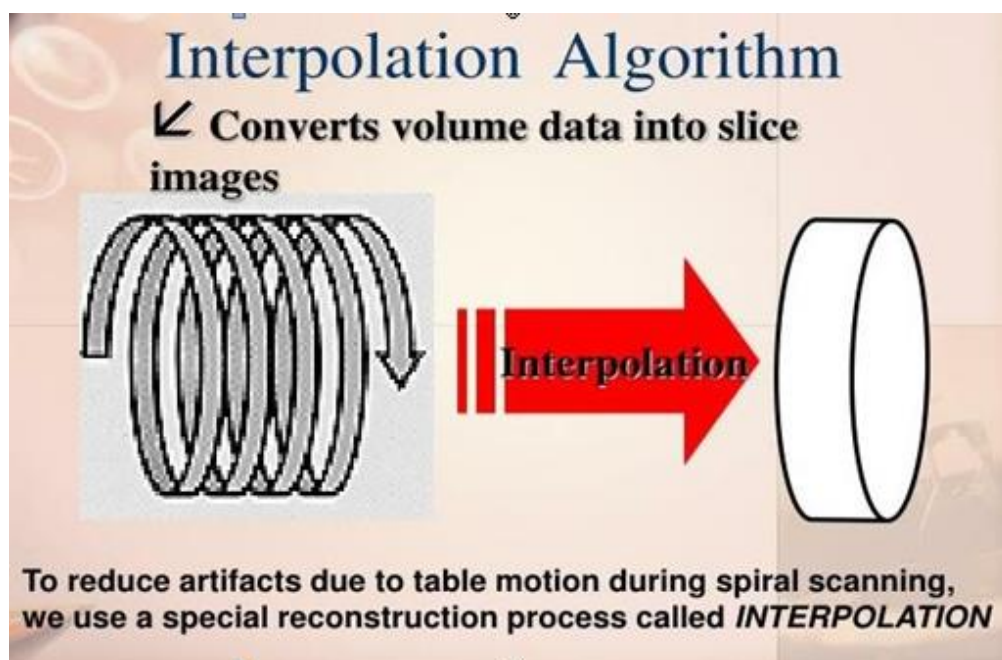
The problem with *continuous tube and table motion* was that *projections precessed in a helical motion* around the patient and *did not lie in a single plane*. This meant that *conventional reconstruction algorithms could not work*.

Helical CT scanning produces a data set in which the X-ray source has travelled in *helical trajectory around the patient*, (the *data are acquired in a helical path* around the patient). Present day CT reconstruction algorithms assume that the X-ray source has *negotiated a circular not a helical path* around the patient. To compensate for these differences in the acquisition geometry, before the actual CT reconstruction *the helical data set is interpolated into a series of planar image data sets* (the reconstruction plane of interest). Interpolation is essentially a *weighted average of the data from either side of the reconstruction plane*, with slightly different weighting factors used for each projection angle.



**Figs.(3): Data interpolation**

***In summary:*** Interpolation Algorithms are the mathematical process required to reconstruct axial images from the spiral volume data set.



## Pitch

During helical scans, the table motion causes *displacement of the fan beam projections along the z axis*; the relative *displacement is a function of the table speed and the beam width*. The *ratio of table displacement per 360° rotation to section thickness is termed pitch*.

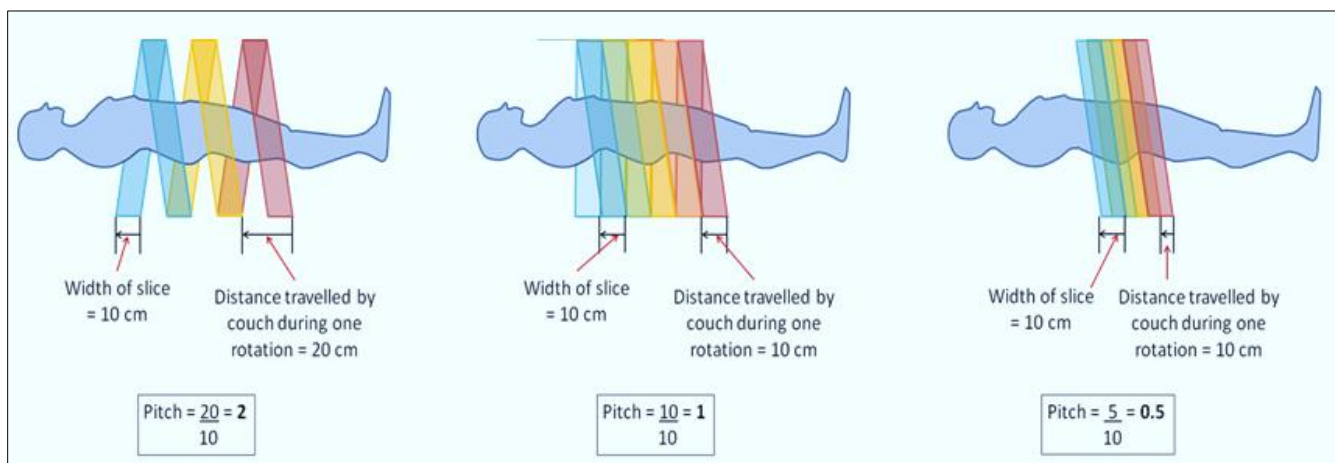
*Pitch is the table movement per rotation divided by beam width.*

$$\text{pitch} = \text{table travel} / \text{beam width}$$

- pitch = 1 - coils of the helix are in contact
- pitch < 1 - coils of the helix overlap
- pitch > 1 - coils of the helix are separated

### For example

- If beam width is 10cm, the table moves 10cm during one tube rotation, then pitch is 1, so, x-ray beam associated with consecutive helical loops are contiguous.
- If beam width is 10cm and table moves 15cm per tube rotation, then pitch is 1.5. So, a gap exists between the x-ray beam edge of consecutive loop.
- If beam width is 10cm and table moves 7.5cm then pitch is 0.75, so, beams and consecutive loops overlap by 2.5 (doubly irradiating the underlying tissues).



**Fig (4): Illustration of pitch concepts**

The relationship between *the volume of tissue imaged and pitch* is given as follows:

**VOLUME IMAGING**

$$\text{Tissue imaged} = \frac{\text{Beam width} \times \text{Pitch} \times \text{Imaging time}}{\text{Gantry rotation time}}$$

**Advantages of helical CT scanner**

- 1) Fast scan times and large volume of data collected.
- 2) Minimizes motion artifacts.
- 3) Less mis-registration between consecutive slices.
- 4) Reduced patient dose.
- 5) Improved spatial resolution.
- 6) Enhanced multiplaner or 3D renderings.
- 7) Improved temporal resolution